# Evaluation of Carbon Dioxide Pressure through Radial Velocity Difference in Arterial Blood Modeled by Drift Flux Model 

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#### Abstract

In this paper, we are interested to determine the carbon dioxide pressure in the arterial blood through radial velocity difference. The blood was modeled as a two phase mixture (an aqueous carbon dioxide solution with carbon dioxide gas) by Drift flux model and the Young-Laplace equation. The distributions of mixture velocities determined from the considered model permitted the calculation of the radial velocity distributions with different values of mean mixture pressure and the calculation of the mean carbon dioxide pressure knowing the mean mixture pressure. The radial velocity distributions are used to deduce a calculation method of the mean mixture pressure through the radial velocity difference between two positions which is measured by ultrasound. The mean carbon dioxide pressure is then deduced from the mean mixture pressure.


Keywords-Mean carbon dioxide pressure, mean mixture pressure, mixture velocity, radial velocity difference.

## I. Introduction

THE arterial blood gas (ABG) analysis consists of a blood sampling by a puncture of the radial artery (systemic artery bringing the oxygenated blood to the hand) and a measurement of three vital parameters which are partial pressure of oxygen $\mathrm{PO}_{2}$, partial pressure of carbon dioxide $\mathrm{PCO}_{2}$ and arterial pH . This allows the evaluation of haemostasis, the confirmation of the respiratory failure diagnosis, and the monitoring of a treatment's effectiveness in the intensive care unit (ICU), pneumology and operating room [1]. The sample Blood is analyzed by electrometric procedures to determine arterial blood pH and $\mathrm{PCO}_{2}$ [2].

ABG analysis is needed for monitoring the respiration of patients under artificial respiration in ICU. Without this information, it becomes hard to physicians to control perfectly the mechanical ventilation. Knowing that the classical sampling process of the arterial blood using a syringe is not only painful for the patient but mostly cannot be repeated frequently. However, frequent blood sampling can cause

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anemia, due to the relatively excessive amount of collected blood (usually 5 to 6 mL per sample including losses), infections and contaminations. Also, it can occasionally cause necrosis due to a decrease or local blockage of blood flow [3]. For all these reasons, a non-invasive method is required to take real time measurements of arterial blood pH and $\mathrm{PCO}_{2}$. This requires necessarily an ex-situ measurement procedure. When it is question to measure a pressure quantity, ultrasounds can be exploited as a safe gas pressures measurement method. The work described in this paper, is interested to procedure determination of the carbon dioxide pressure.
The setting of the measurement procedure firstly needs a mathematical modeling of the arterial blood. In this case, the blood solution is modeled as an incompressible Newtonian mixture of two phases. Mainly, it is about an aqueous carbon dioxide solution with carbon dioxide gas. The suitable model to describe the flow of this mixture is Drift flux model. The Drift flux and the Young-Laplace equations are used to simulate the fluid flow and to deduce the carbon dioxide pressure when calculating the mixture radial velocity [4]. In this paper, the method used for the assessment of mean carbon dioxide pressure is based on the determination of radial velocity distributions.

## II.Methods and Materials

## A. Mathematical Model

The arterial blood contains various cells in plasma solution (water) which are red blood cells, white blood cells and platelets as well as gases including carbon dioxide and oxygen. Since the work is interested to determine the carbon dioxide pressure, the considered fluid is modeled as a two phase mixture flowing in a rigid canalization by the Drift flux model. It is about a gas phase (microbubbles of carbon dioxide) and a liquid phase (aqueous carbon dioxide solution) [4].
The drift flux model considers the whole mixture taking into account a drift velocity between the gas phase (dispersed phase) and the liquid phase (continuous phase). Experimentally, the measurement of the mixture velocity permits to deduce another characteristic of the two phases especially the gas phase. Both phases are considered to be incompressible. The first three equations of the considered model are used to express the mass and momentum conservations as

1) Mixture continuity equation

$$
\begin{equation*}
\nabla .\left(\rho_{m} U_{m}\right)=0 \tag{1}
\end{equation*}
$$

2) Continuity equation for dispersed phase

$$
\begin{equation*}
\nabla \cdot\left(\alpha_{2} \rho_{2} U_{m}\right)=-\nabla \cdot\left(\frac{\alpha_{2} \rho_{1} \rho_{2}}{\rho_{m}} V_{2 j}\right) \tag{2}
\end{equation*}
$$

3) Mixture momentum equation

$$
\nabla \cdot\left(\rho_{m} U_{m}\right)=-\nabla p_{m}+\nabla \cdot(\tau)+\rho_{m} g_{m}-\nabla \cdot\left(\frac{\alpha_{2}}{1-\alpha_{2}} \frac{\rho_{1} \rho_{2}}{\rho_{m}} V_{2 j} V_{2 j}\right)
$$

where, $U_{m}$ : mixture velocity, $\rho_{m}$ : mixture density, $\rho_{l}$ : liquid density, $\rho_{2}$ : gas density, $\alpha_{2}$ : volumetric fraction of gas, $p_{m}$ : mixture pressure, $\tau$ : viscous stress, $g_{m}$ : gravitational acceleration vector, $V_{2 j}$ : drift velocity vector of the gas phase [5].

The mixture pressure is expressed by the liquid pressure and the gas pressure as:

$$
\begin{equation*}
p_{m}=\alpha_{1} p_{1}+\alpha_{2} p_{2} \tag{4}
\end{equation*}
$$

$\alpha_{l}$ presents volumetric fraction of liquid phase, $p_{l}$ presents liquid pressure, and $p_{2}$ presents gas pressure.
Equations (1)-(3) permit to determine distributions of mixture velocities, the volumetric fraction of gas, and mixture pressure [4]. Equation (4) allows to relate pressures of gas and liquid phases to the mixture pressure but it is not sufficient to calculate the carbon dioxide pressure. To evaluate the gas pressure distribution, it is necessary to use a fifth equation. This equation is needed to determine the mentioned pressure distribution, knowing the mixture pressure distribution and the phase fractions. Then, the Young- Laplace equation is used to correlate the pressures of the two phases (5). The considered equation is written as:

$$
\begin{equation*}
p_{2}-p_{1}=\frac{2 \sigma}{R} \tag{5}
\end{equation*}
$$

The term $\sigma$ presents the surface tension and the term $R$ presents the radius of the microbubble of the gas [6], [7].

Then, the use of the two later equations (4) and (5) allows the assessment of gas pressure distribution through the mixture pressure and velocities.

## B. Calculation Method

For a given fixed initial conditions, the resolution and the numerical simulations of (1)-(5) permit to calculate the spatial distribution of the three velocity's components $U_{x m}, U_{y m}$, and $U_{z m}$ respectively along x axis (flow axis), y axis, and z axis, as well as the spatial distribution of the mixture pressure $p_{m}$ and carbon dioxide pressure $p_{2}$. This constitutes the first step of the study [4].

The theoretical results allow understanding of the behavior and the characteristics of the considered mixture. Through
these results, a calculation method is established to determine the mean gas pressure in the mixture knowing the mean mixture pressure. The later parameter is deduced from the mixture radial velocity distribution.
The blood sampling is done orthogonally to the flow axis, to avoid the effect of the heart pressure. Inspired by this technique, the mean carbon dioxide pressure is calculated by the radial velocity distribution values. Practically, mean gas pressure is determined through mean mixture pressure. According to (3), the mixture velocity values ( $U_{z m}, U_{y m}$, and $U_{x m}$ ) depend on mixture pressure $p_{m}$. Thus, several distributions of $U_{z m}$ in ( $\mathrm{x}, \mathrm{z}$ ) plan are calculated for different values of mean mixture pressure. These later values are calculated by the integration of pressure values in all canalization's cells.
In practice, ultrasound is exploited in Doppler technique for measurement of linear blood flow. In this case, it is concevable to use two ultrasonic probes fixed on the canalization perpondicularly to the flow direction. Both probes must be relatively one far from the other to avoid measurement errors. In these positions, probes are able to measure the radial velocity of the mixture in each point on the probes fields of view. This method permits to deduce the mean mixture pressure knowing the radial velocity difference values between the two considered directions as

$$
\begin{equation*}
P_{\text {moy }}=f\left(\Delta U_{z m}\right) \tag{6}
\end{equation*}
$$

## C. Calculation

The numerical simulations of the mixture parameters are made by MATLAB. Therefore, the calculation permits the assessment of the mean mixture pressure and the mean carbon dioxide pressure through the differences of radial velocity distributions.

## III. Results and Discussion

The fluid moves horizontally through a cylindrical rigid canalization with constant cross-section ( 4 mm radius and 10 cm length). Samples of the velocities $U_{z m}, U_{y m}$, and $U_{x m}$ are chosen respectively as $9 \times 9 \times 10,9 \times 10 \times 9$, and $10 \times 9 \times 9$ in the xyz space. Numerical simulations of the mixture allowed to calculate the distribution of radial velocity $U_{z m}$ for different values of mean mixture pressure $P_{\text {moy }}$.
The calculation of velocity distributions $U_{z m}$ along x axis for different values of $z$ between 2 and 9 and different values of mean mixture pressure between 3.2 and 8.8 kPa , gives families of curves (Fig. 1) that changes remarkably with $z$ position, but they are also shown coherence in the x interval between 3 and 8 . In fact, in this interval, all the curves are continuous and differentiable. Then, from the curve families presented in Fig. 1, new curve families are deduced expressing the mean mixture pressure through the velocity distribution $U_{z m}$ (Fig. 2).


Fig. 1 Distribution of $U_{z m}$ with different values of $P_{m o y}$ at different z positions

Contrary to the first families of curves (Fig. 1), the second families show independent and generally linear curves which can give options to deduce calculation methods of mean
mixture pressure by ultrasound measurement of radial velocity $U_{z m}$. Practically, it is not suitable to do simultaneous measurements of velocities in all considered positions along
the x axis (from the first position to the ninth last position) because of confusion in ultrasound detection when two probes are nearby. This can constitute a source of measurement errors. To circumvent this difficulty, it is advisable to calculate


Fig. 2 Distribution of $U_{z m}$ with $P_{\text {moy }}$ for different x positions

Then, the radial velocities differences are calculated between positions 3 and 8 on the x axis for the z positions ( z axis presents the radial axis) from 2 to 9 (Fig. 3). Thus, it is
possible to use two ultrasonic probes put on the two considered x positions and measure radial velocity.

The radial velocity's differences calculated between these
two positions is relatively important and then measurable. Fig. 3 represents the distribution of radial velocity's differences with different values of mean mixture pressure from the second position to the ninth position along z axis. Every curve corresponds to the variation of $P_{m o y}$ with the difference of $U_{z m}$ for a z position (away from the center and boundary). At the beginning, the function $P_{\text {moy }}=\mathrm{f}\left(\Delta U_{z m}\right)$ takes a linear profile for the first positions then the profile becomes increasingly nonlinear while approaching the walls. This nonlinearity is caused by the effects of boundaries on the mixture velocity.


Fig. 3 Distribution of $U_{z m}$ difference between $\mathrm{x}=3$ and $\mathrm{x}=8$ with $P_{\text {moy }}$ at z positions

According to the results shown in Fig. 3, it is appropriate to determine the mean mixture pressure using linear curves. For this, the functions $P_{m o y}=\mathrm{f}\left(\Delta U_{z m}\right)$ for $\mathrm{z}=2,3$, and 4 are established mathematically by linear fittings as $P_{m o y}=\mathrm{a} \Delta U_{z m}+\mathrm{b}$. After comparison between the curves and fittings (Fig. 4), it turns out that only curves related to both $\mathrm{z}=2$ and $\mathrm{z}=3$ are linear and the linearity starts to disappear since $z=4$. Then, the mean mixture pressure is calculated with radial velocity's difference in positions $\mathrm{z}=2$ and $\mathrm{z}=3$. The two linear curves of positions $\mathrm{z}=2$ and $\mathrm{z}=3$ are described by the following linear equations:

For position $\mathrm{z}=2$ :

$$
\begin{equation*}
P_{\text {moy }}=-7.6685 e^{06} \Delta U_{z m}+0.0371 e^{06} \tag{7}
\end{equation*}
$$

For position $\mathrm{z}=3$ :

$$
\begin{equation*}
P_{\text {moy }}=-4.8493 e^{06} \Delta U_{z m}+0.0471 e^{06} \tag{8}
\end{equation*}
$$

The calculated function at radial positions $\mathrm{z}=2$ and $\mathrm{z}=3$ will be operated to define the mean mixture pressure. The first function will be used to measure the $P_{\text {moy }}$ and the second one will be employed to verify the measured value of $P_{\text {moy }}$.

Equations (4) and (5) relate to the mean gas pressure $P_{\text {gmoy }}$ to the mean mixture pressure. Fig. 5 shows the variation $P_{g m o y}$ with the $P_{\text {moy }}$. This will be able to determine the mean carbon dioxide pressure in the mixture through the difference of radial velocity.


Fig. 4 Superposition of real curves and fittings of $U_{z m}$ difference at $\mathrm{z}=2, \mathrm{z}=3$, and $\mathrm{z}=4$


Fig. 5 Variation of $P_{\text {gmoy }}$ with $P_{\text {moy }}$

## IV. Conclusion

The arterial carbon dioxide pressure presents an indispensable parameter to control the mechanical ventilation of patients in ICUs. To measure this parameter in a noninvasive way, the arterial blood was modeled by the Drift flux model that relates the fluid velocity and the fluid pressure and the Young-Laplace equation that involves the gas pressure. The numerical simulations of this model were exploited to the calculation of mixture radial velocity distribution in $x$ and $z$ positions with different values of mean mixture pressure $P_{\text {mov }}$. These distributions allow to determine the calculation methods of mean mixture pressure by ultrasound measurement of radial velocity $U_{z m}$ at different z and x positions. To make this method practical, it is suitable to determine the mean mixture pressure through radial velocity differences along z axis at two x positions. The use of two probes permits to avoid measurement errors due to the confusion in ultrasound detection. According to the calculated distribution of $U_{z m}$ differences between the two considered x positions, two linear
curves are chosen to determine the mean mixture pressure at $\mathrm{z}=2$ and $\mathrm{z}=3$. The fitting of these curves are realized as $P_{m o y}=\mathrm{a} \Delta U_{z m}+\mathrm{b}$. Then, these functions are used to determine $P_{\text {moy }}$ through measured radial velocity differences and consequently to deduce the mean carbon dioxide pressure.

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